

# Polymerization Synthetic polymers in dentistry

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# Types of dental materials

- Metallic materials - denture frameworks, supraconstructions, implants, orthodontic brackets, wires, amalgams.
- Inorganic materials - cements, dental ceramics, gypsum products, investment materials.

- Organic (polymer-based) materials

# Types of polymer materials in dentistry

- Natural polymers - guttapercha (obturation points), polysaccharides agar, alginate (impression materials).

- Synthetic polymers - methacrylate-based polymers, silicone polymers, epoxies, etc.

## WHY?

Easily modified to prepare **tailor-made materials with good mechanical and acceptable biologic properties**

# Typical applications of polymer-based materials in dentistry

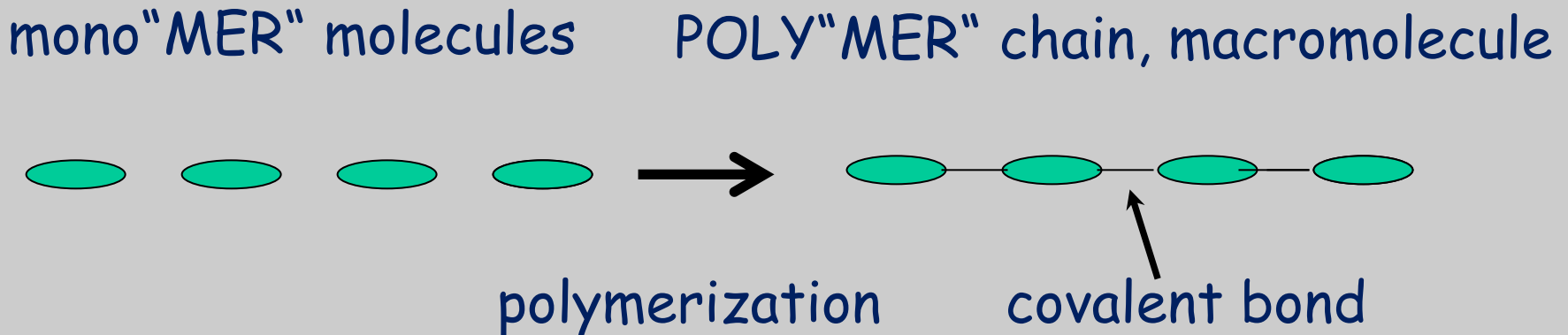
- Dentures (bases, artificial teeth, orthodontic appliances).
- Filling materials (composites, cements, adhesives).
- Root canal sealers (endodontics).
- Impression materials.
- Equipment (spatulas, measures, curing units, etc.).

# What we are going to discuss?

- Terms and definitions.
- Structure of polymer chains.
- Polymerization reactions.
- Methyl methacrylate polymers.
- Typical methacrylate monomers in dental materials.
- Other polymers used in prosthetic dentistry.

# Definition

Polymer - a chemical compound composed of large molecules „MACROMOLECULES“ formed by union of many „POLY“ small repeating units „MER“.



Note:

## In stomatology

Polymers = sometimes named resins

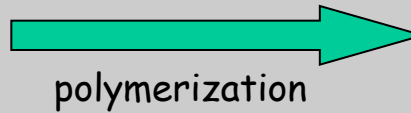
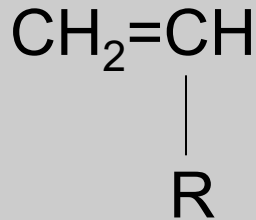
but:

Some monomers – (dimethacrylates) are frequently mentioned also as resins, e.g. resin composites (instead of polymer composites used technical terminology)

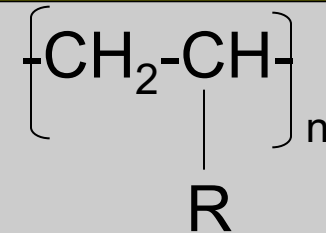
# What controls polymer properties?

## 1. Chemical composition and structure of monomer/s

Vinyl monomers



Structure of vinyl polymers

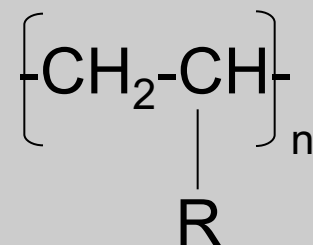
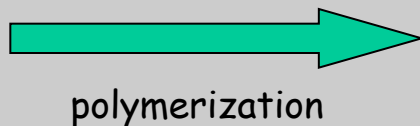
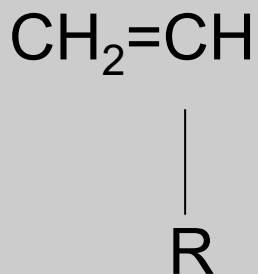


Examples:

R = H: polyethylene - a hydrophobic, semicrystalline polymer

R = OH: poly(vinyl alcohol), a hydrophilic water soluble polymer with gelling properties due to H-bonds



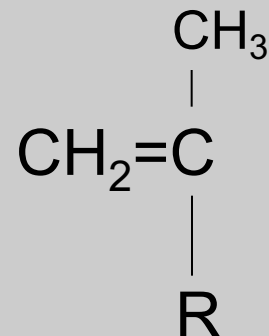
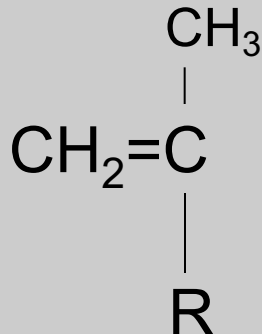


$\text{R} = \text{COOH}$  - acrylic acid

Water soluble

$\text{R} = \text{COOH}$  - polyacrylic acid

Water soluble



$\text{R} = \text{COOH}$  - methacrylic acid/polymethacrylic acid

Partly water soluble

$\text{R} = \text{COOCH}_3$  - methyl methacrylate/polymethylmethacrylate

Insoluble in water

If one type or different monomers are linked together:

One monomer - HOMOPOLYMERS

Two or three monomers - COPOLYMERS

## 2. Topology of polymer chains

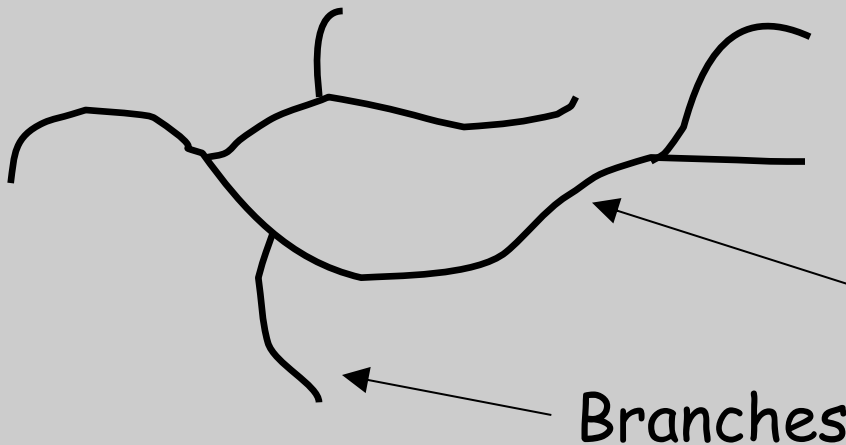


Linear polymers

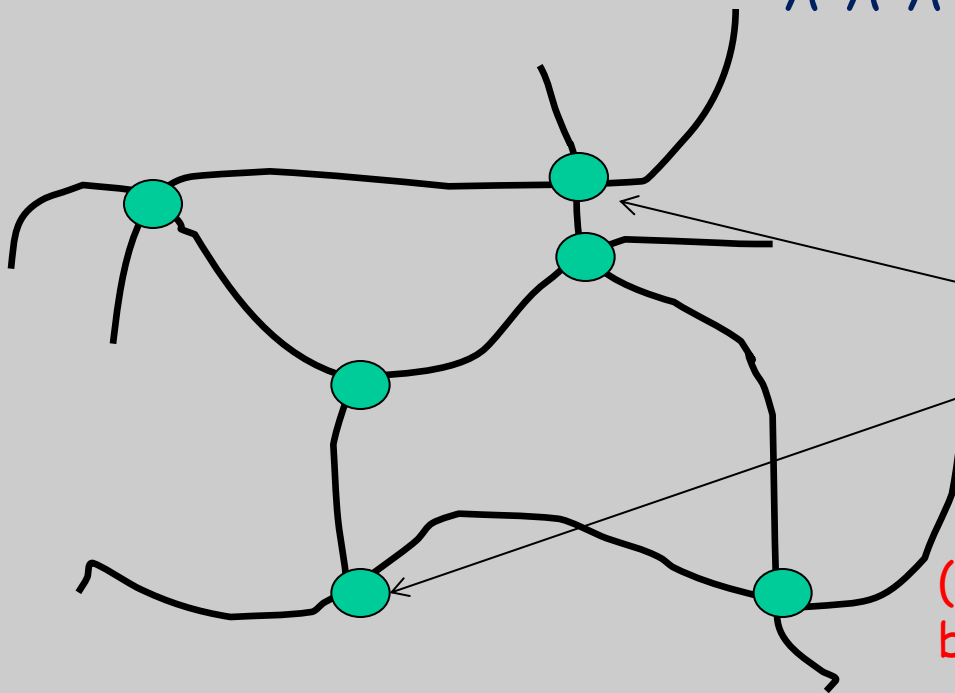
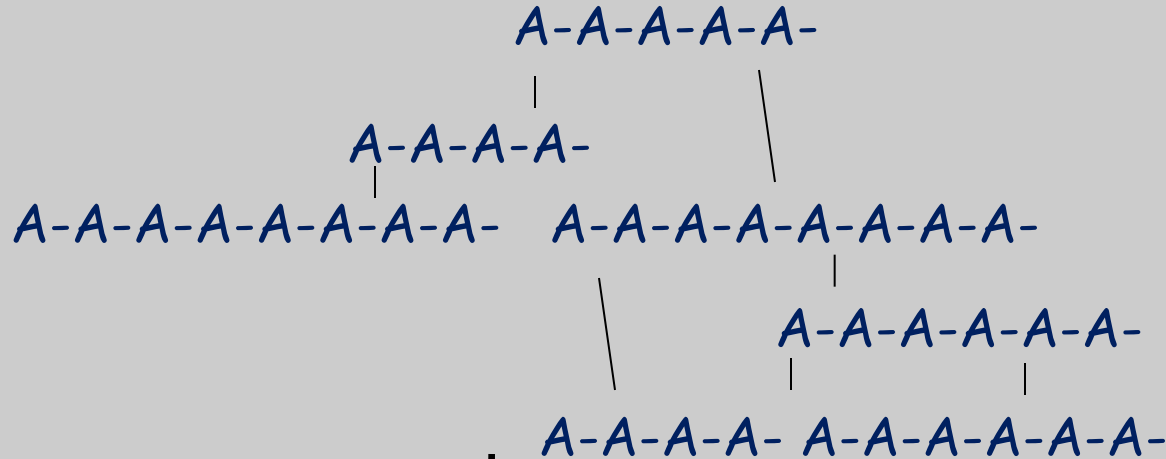
(monomers with one double bond)

Nonlinear (branched) polymers

(monomers with two/more double bonds at their lower concentration)



- Cross-linked polymer (polymer networks)



Cross-links (permanent connections between chains) restrict motion of chains → rigidity

(monomers with two/more double bonds at their higher concentration)

# Cross-links strongly affect mechanical properties and thermal behaviour of polymers

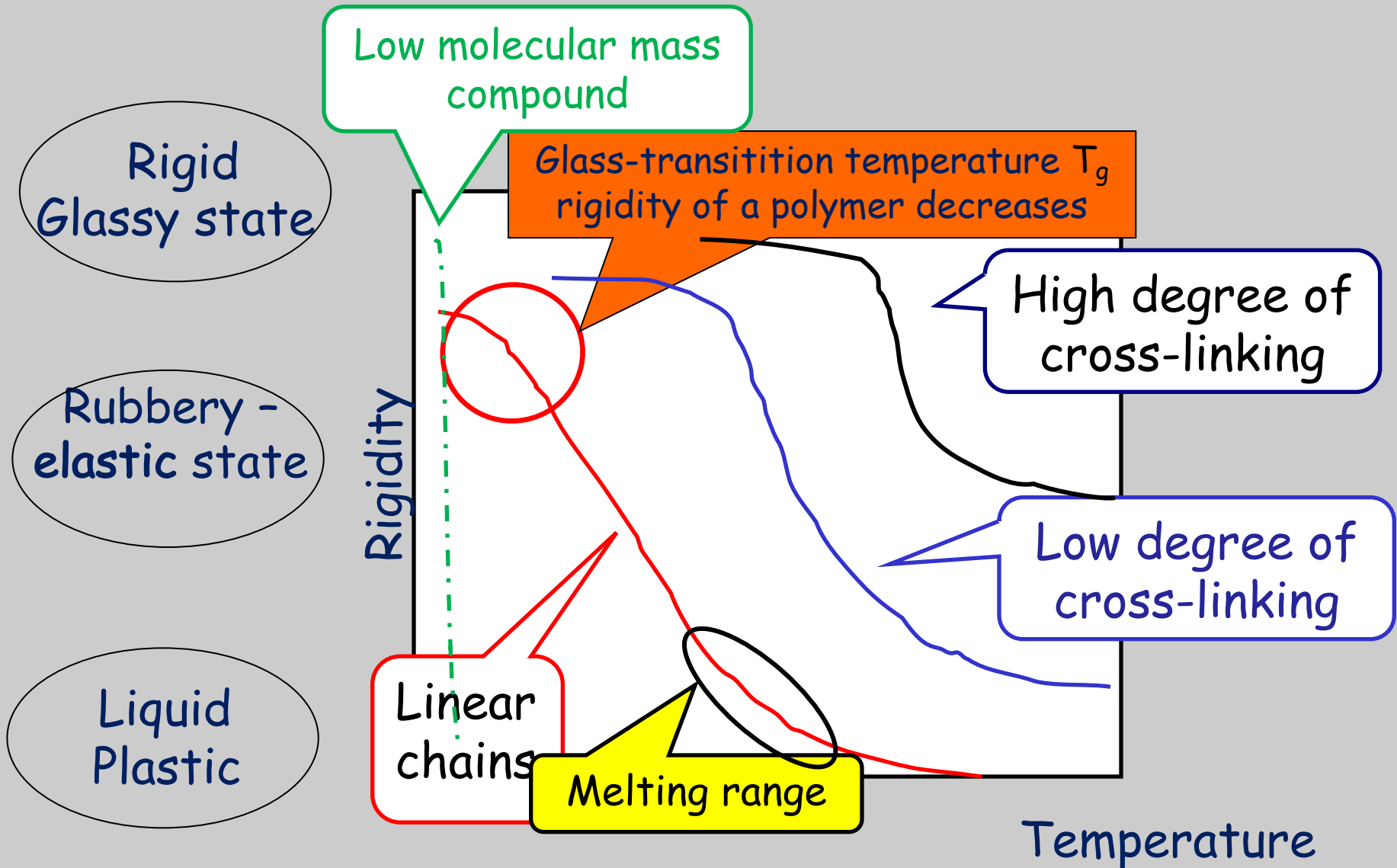
Linear or branched polymers - flow when heated, can be easily reshaped upon heating, usually soluble in organic solvents

- thermoplastic polymers

Cross-linked polymers - they can not be reshaped on heating, do not melt, but decompose on heating, insoluble in organic liquids,

- thermosetting polymers

# Thermal behaviour of polymers



### 3. Monomer distribution in copolymers

A-B-A-B-B-B-A- *statistical (random)*

A-B-A-B-A-B-A- *alternating*

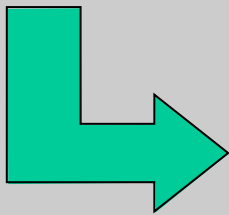
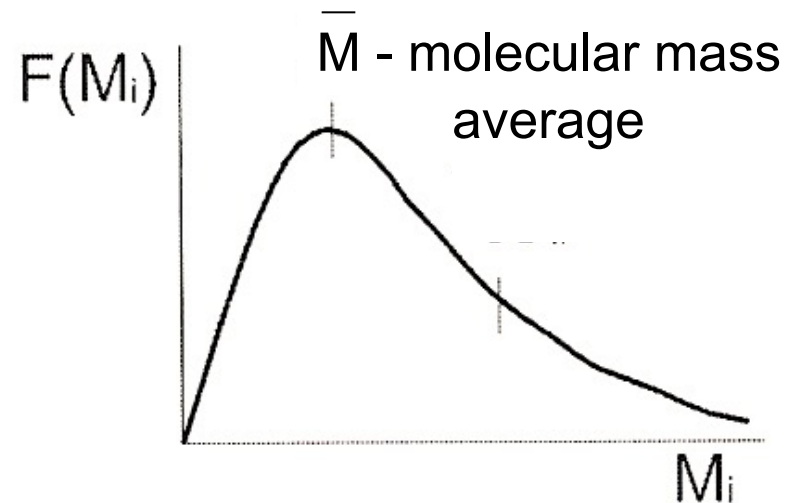
A-A-A-B-B-B-B-A-A- *block*

          -A-A-A-A-A- *graft/branched*  
          |  
-B-B-B-B-B

## 4. Polymer molecular mass

Simple compounds -  
formed from identical  
molecules

Molecules of polymer -  
strongly differ (vary by  
many monomer units in  
macromolecules)



Polymers are characterized by  
molecular mass/polymerization  
degree average



# Principal requirements on polymer materials in dentistry

1. **Fast** polymerization,

2. high molecular weight - (improved **mechanical properties**, e.g. strength, hardness, resistance to wear, oral cavity environment, etc.),

3. acceptable biologic properties - decreased **leachable** components.

# Synthetic polymers

Prepared via polymerization reactions:

- **Chain-growth** (addition) polymerization  
most often free radical polymerization of monomers with **double bonds**.
- **Step-growth polymerization** (e.g. polycondensation) of **di/more functional monomers**  
**frequently** with **release of low molecular compounds**  
(analogous reaction to low molecular weight compounds).

# Types of chain-growth polymerizations:

- Free radical polymerization - active centre is a free radical (with an unpaired electron).
- Cationic polymerization - active centres bear positive charge.
- Anionic polymerization - active centres bear negative charge.

# Free radical polymerization

## Characteristics

- Starts from an active center (e.g free radical) only these molecules are capable to react.
- $\pi$ -bond of monomer is converted to  $\sigma$ -bond in the polymer chain.
- Monomer molecules add sequentially to the end of a growing chain.
- Is very fast and exothermic.
- Produces high molecular mass polymers.
- Free-monomers are present.

# Step-growth polymerization used less often in dentistry

## Types of step-growth polymerization

- Polycondensation
- Polyaddition

# Step-growth polymerization

## Characteristics

- Proceeds by conventional functional group reactions (condensation, addition).
- Needs at least 2 functional groups per reactant.
- Any monomer molecule has the „same“ probability to react.
- After an elementary reaction - ability to grow remains.
- Polymers are formed more slowly than by free radical polymerization.

- The chain ends remain active.

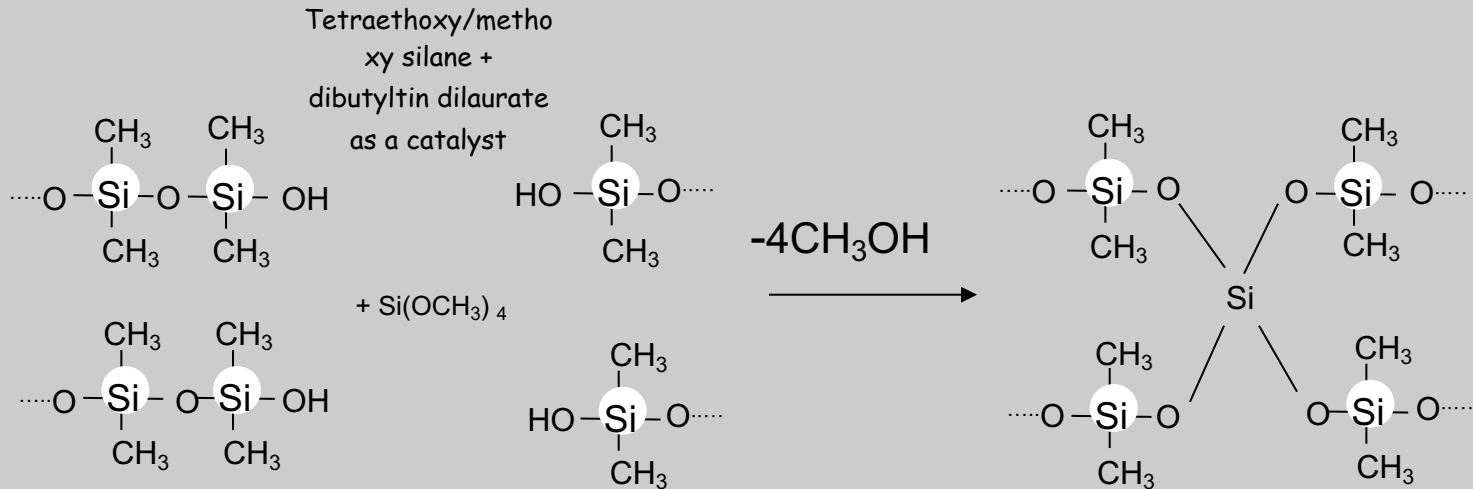
- Polymers are generally of lower molecular mass.

- Dimers, trimers or oligomers are present while concentration of free monomers rapidly decreases.

- A small molecular weight products are frequently released (polycondensation) - inhibit polymerization.

# 1. Polycondensation cross-linking

## Setting reaction of C-silicone impression materials

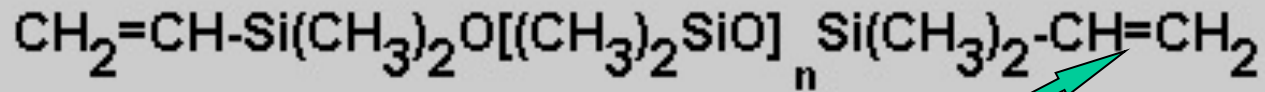


Hydroxyterminated dimethylsiloxane prepolymers



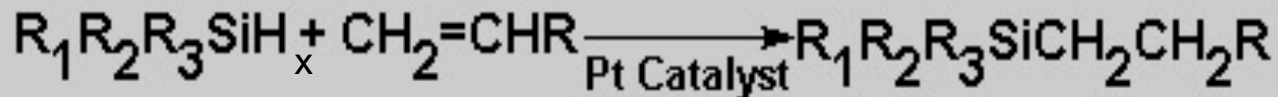
## 2. Polyaddition

Setting reaction of A-silicone impression materials



Vinyl terminated siloxane oligomer

Addition of -H on vinyl double bond



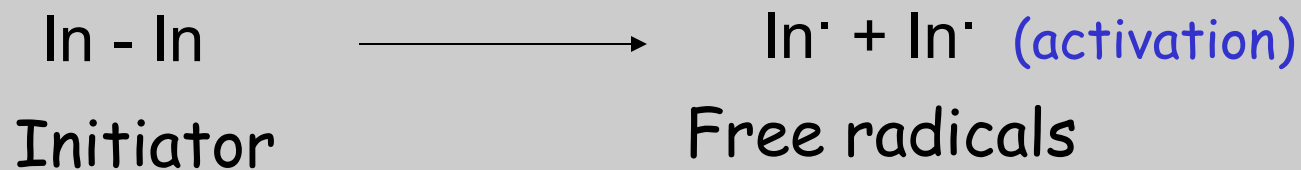
methylhydrosiloxane oligomers - a cross-linking agent

# Free radical polymerization mechanism

# Stages of free radical polymerization

## 1. Initiation/induction - process starts

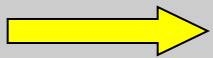
- Primary radical formation

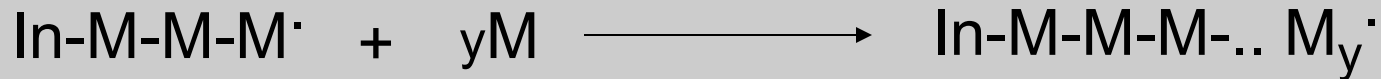
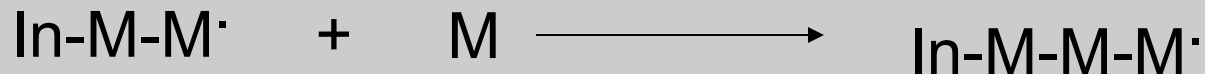
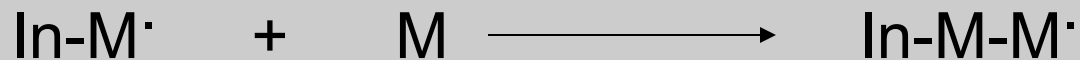


- Addition of primary radical on the double bond of monomer



the chain  
growth starts

2. Propagation - addition of monomer molecules to the active center  a polymer chain is growing



3. Termination - the growing chain is stopped

- Radical coupling/recombination (most common)



- Chain transfer - an active centre is split off from the growing chain with a special molecule, terminating the chain growth and starting a new chain - control of molecular mass.

## 1. Original chain terminates



## 2. New chain growth starts



## Special cases of chain transfer reactions:

A retarder is a substance that reacts with a growing chain forming **less reactive** radical B· and thus making polymerization rate „**slow**“.

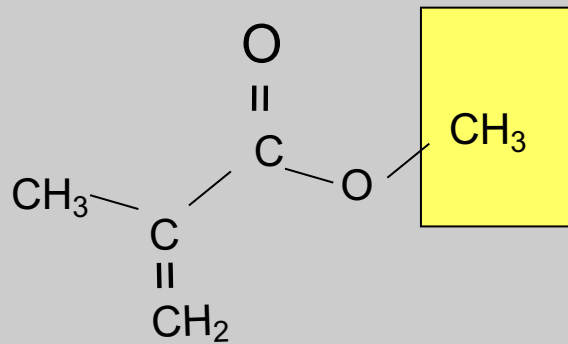
An inhibitor is a substance that reacts with an active radical to form **stable** compound unable addition to monomer - completely **stops** “inhibits” polymerization.

The most important polymerization route in dentistry is free radical polymerization of methacrylate monomers:

- Preparation of methacrylic polymers (dentures, artificial teeth, relining materials, orthodontic appliances...).
- Setting reaction of dimethacrylate and other multifunctional based dental materials (composites, adhesive systems, glass-ionomer cements...).

# Methyl methacrylate (MMA) polymers

Most frequently used group of polymers in prosthetic and orthodontic dentistry



methyl methacrylate (MMA)

**Why?** Because these materials can be easily adopted to individual purposes (dentures, teeth), polymerization is fast and the polymers are usually well accepted by the human body



# Properties of MMA

- Colorless liquid
- Immisible with water but with organic solvents
- Melting point  $-48^{\circ}\text{C}$
- Boiling point  $100.3^{\circ}\text{C}$
- Density  $0.945 \text{ g/mL}$
- Heat of polymerization  $54.3 \text{ kJ/mol}$   
(!! exothermic reaction !!)
- Irritant
- !! Flamable !!

## Properties of poly(methyl methacrylate) - PMMA

- Transparency and high clarity,
- Compression strength 90 - 100 MPa,
- Very rigid - elastic modulus above 2.4 GPa,
- Water sorption up to app. 1.0 wt %,
- Temperature resistance  $T_g = 120 - 125^\circ\text{C}$ ,
- Soluble in organic solvents (MMA, acetone, toluene etc).

**Density 1.19 g/cm<sup>3</sup> (causes polymerization contraction /shrinkage app. 22 vol %)**

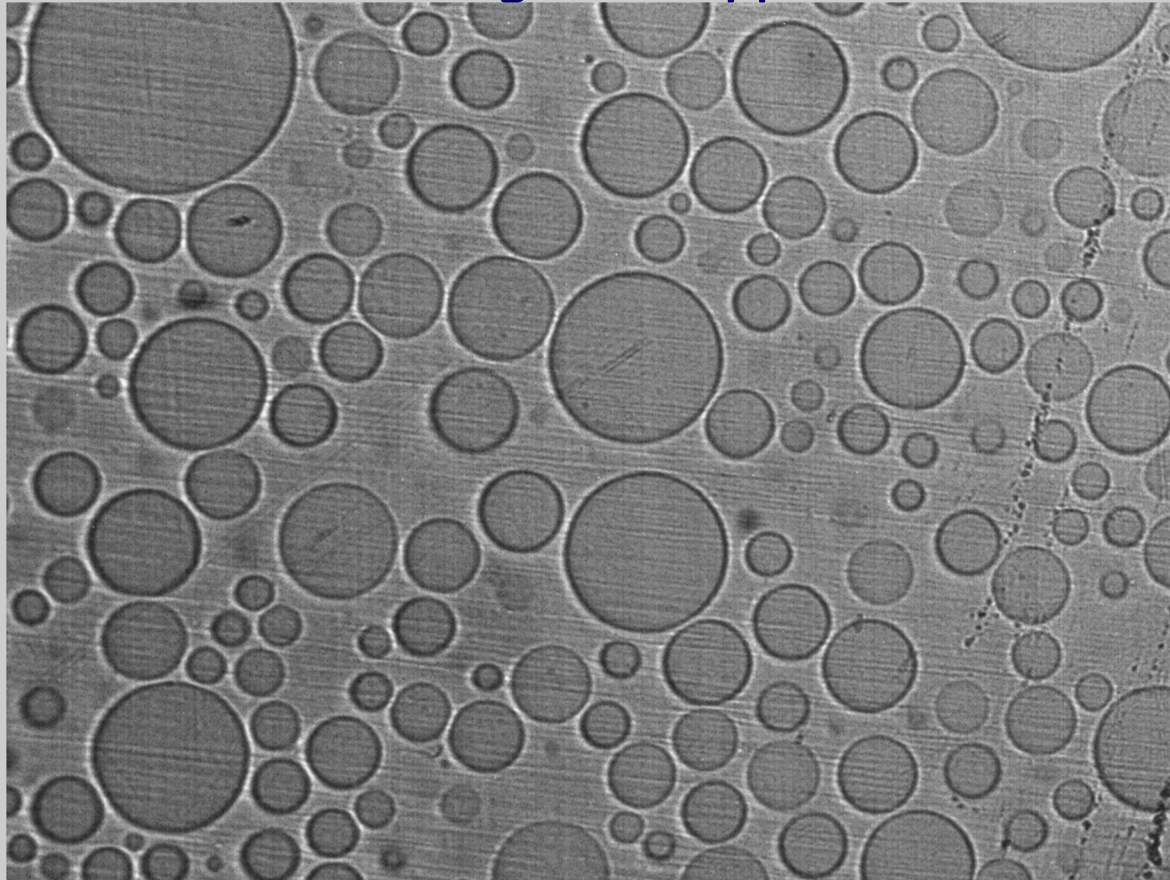
Main problem - how to overcome  
polymerization shrinkage ????

Leading to pronounced inaccuracy  
of dental reconstructions

- First applications in denture preparation was via compression moulding of molten PMMA (too expensive and complicated)
- 1936 - Kulzer: powder/liquid system
  - Powder - PMMA prepolymer with residues of the initiator (dibenzoyl peroxide - DBP)
  - Liquid - MMA monomer and additives
  - When mixed together a workable - plastic mass (dough) is formed and polymerized in individually fabricated mould
  - Decreased polymerization shrinkage (app. 6 vol %) at powder/liquid ratio 3-2.6/1

# PMMA prepolymer beads

Prepared by suspension polymerization in an aqueous media and using DBP type initiators



Average particle size 0.005-0.100 mm

# Classification of methyl methacrylate polymers according to initiation reactions

- Heat activated (heat cured/heat curing) resins,
- Chemically activated (self cured/curing, cold curing, autopolymerizing, fast curing) resins.

# Heat activated resins

(denture base resins, resins for artificial acrylic teeth, crown and bridge polymers)

Composition:

**powder:** PMMA prepolymer with dibenzoyl peroxide  
(in the PMMA beads, 0.5 - 0.6 wt %)

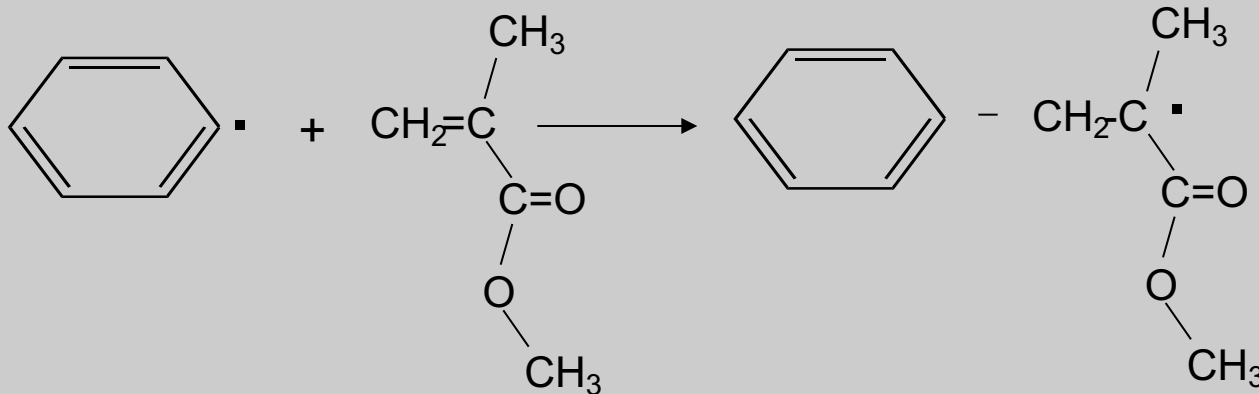
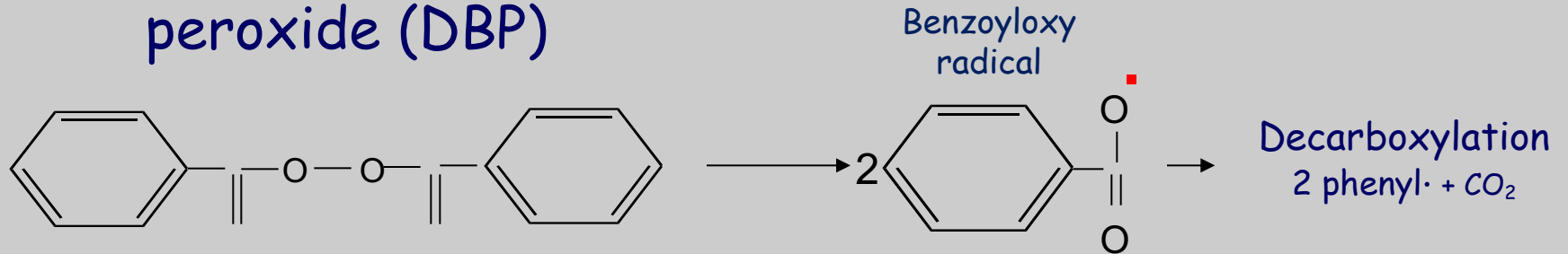
**liquid:** MMA, cross-linking agent (app. 1 - 6 wt %),  
inhibitors, additives (plasticizers)

Volume mixing ratio (powder/liquid): 3-2.5/1.0

# Polymerization scheme

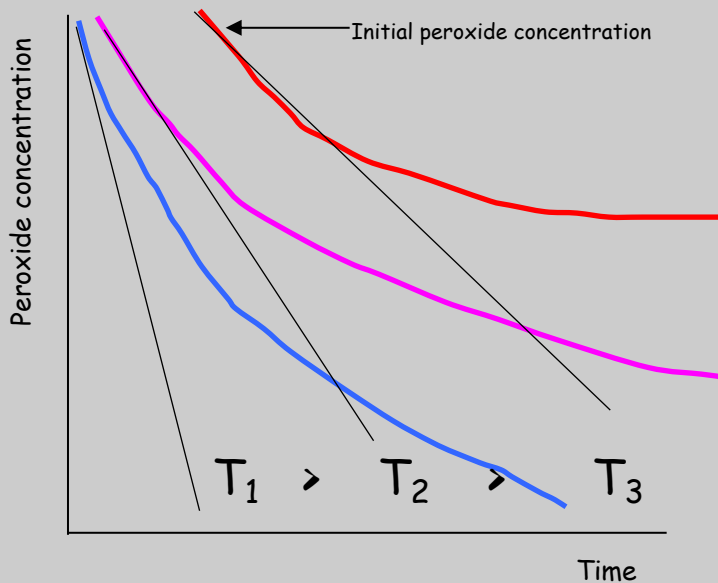
- Initiation

- Thermal decomposition of residual dibenzoyl peroxide (DBP)





# Thermal decomposition of DBP



$$C_t = C_0 \cdot e^{-kt}$$

$C_t$  = concentration of peroxide at time  $t$

$k$  = kinetic constant (slope)

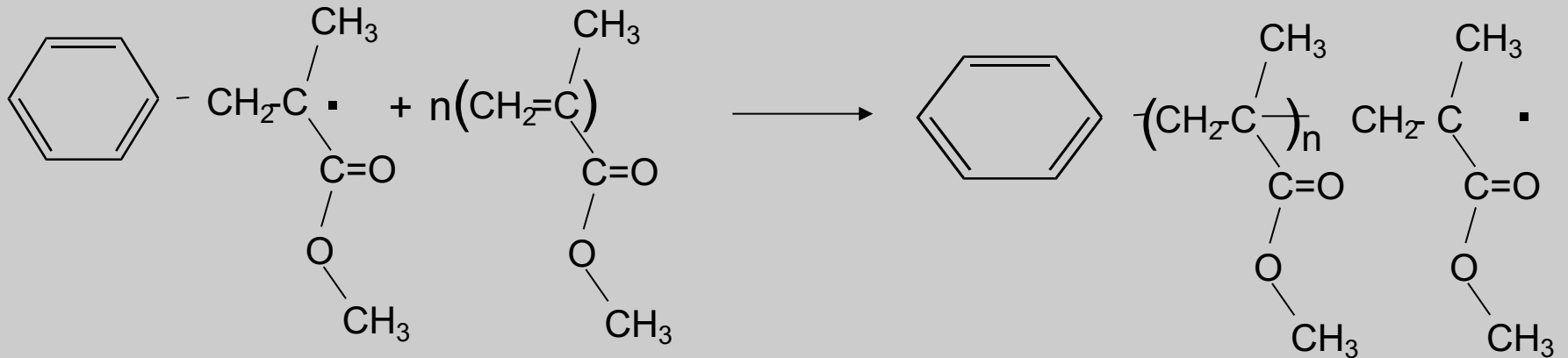
$t$  = time

## Effect of temperature

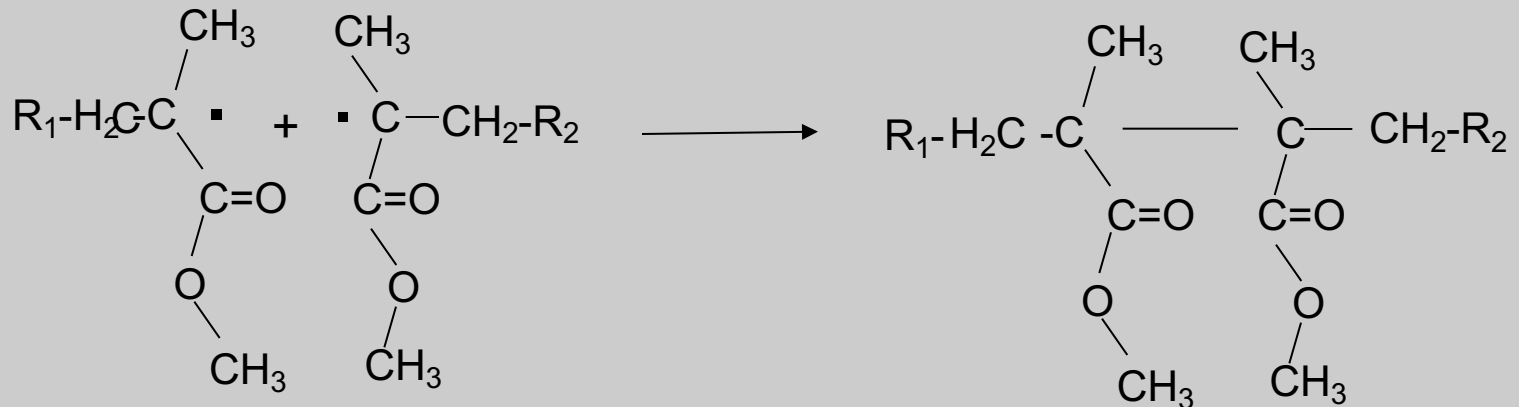
The temperature dependence of kinetic constant is given by the Arrhenius law:

The higher temperature - increased concentration of radicals (an increased rate of peroxide decomposition) and higher polymerization rate

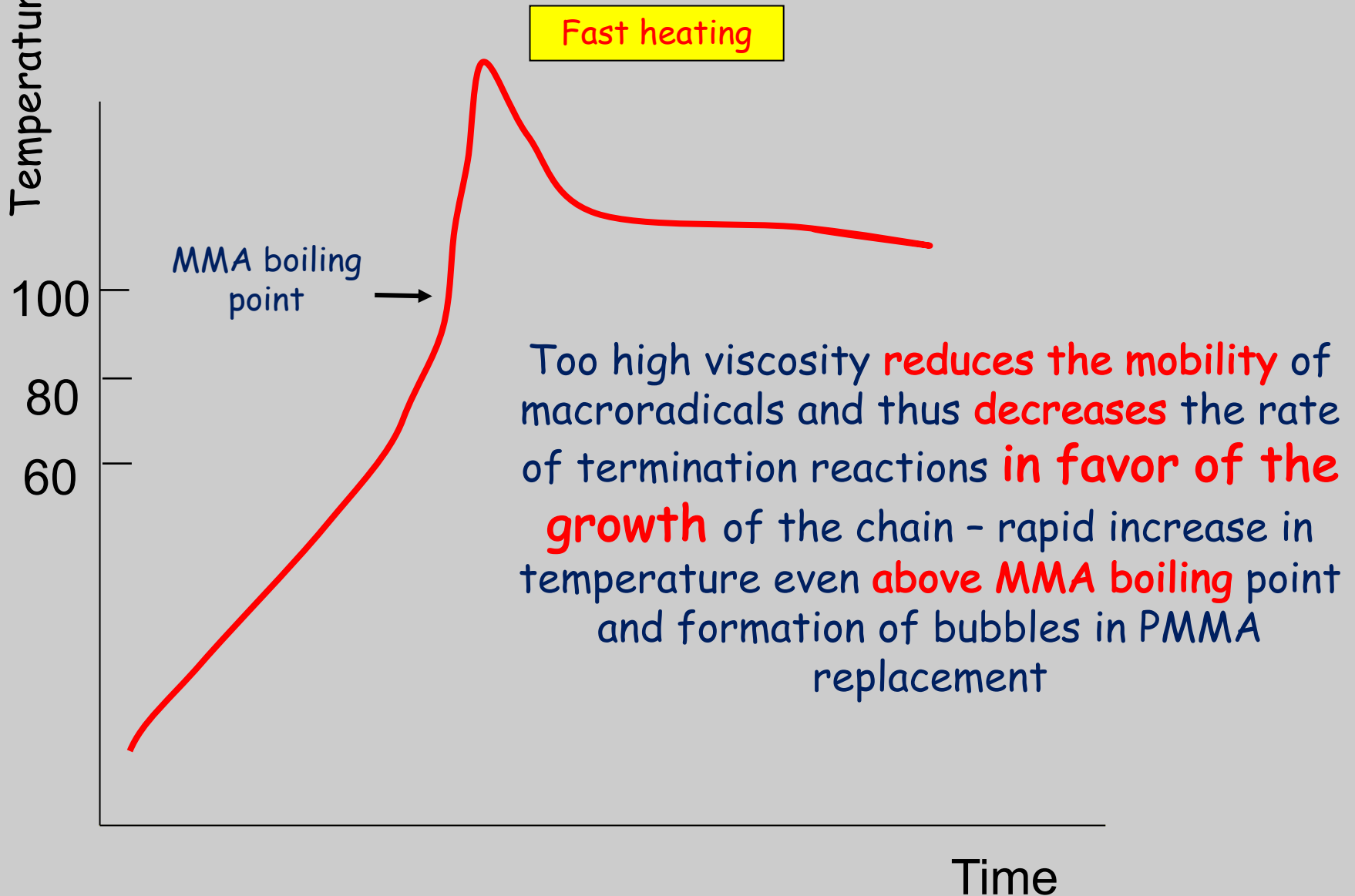
# • Propagation



# • Chain termination

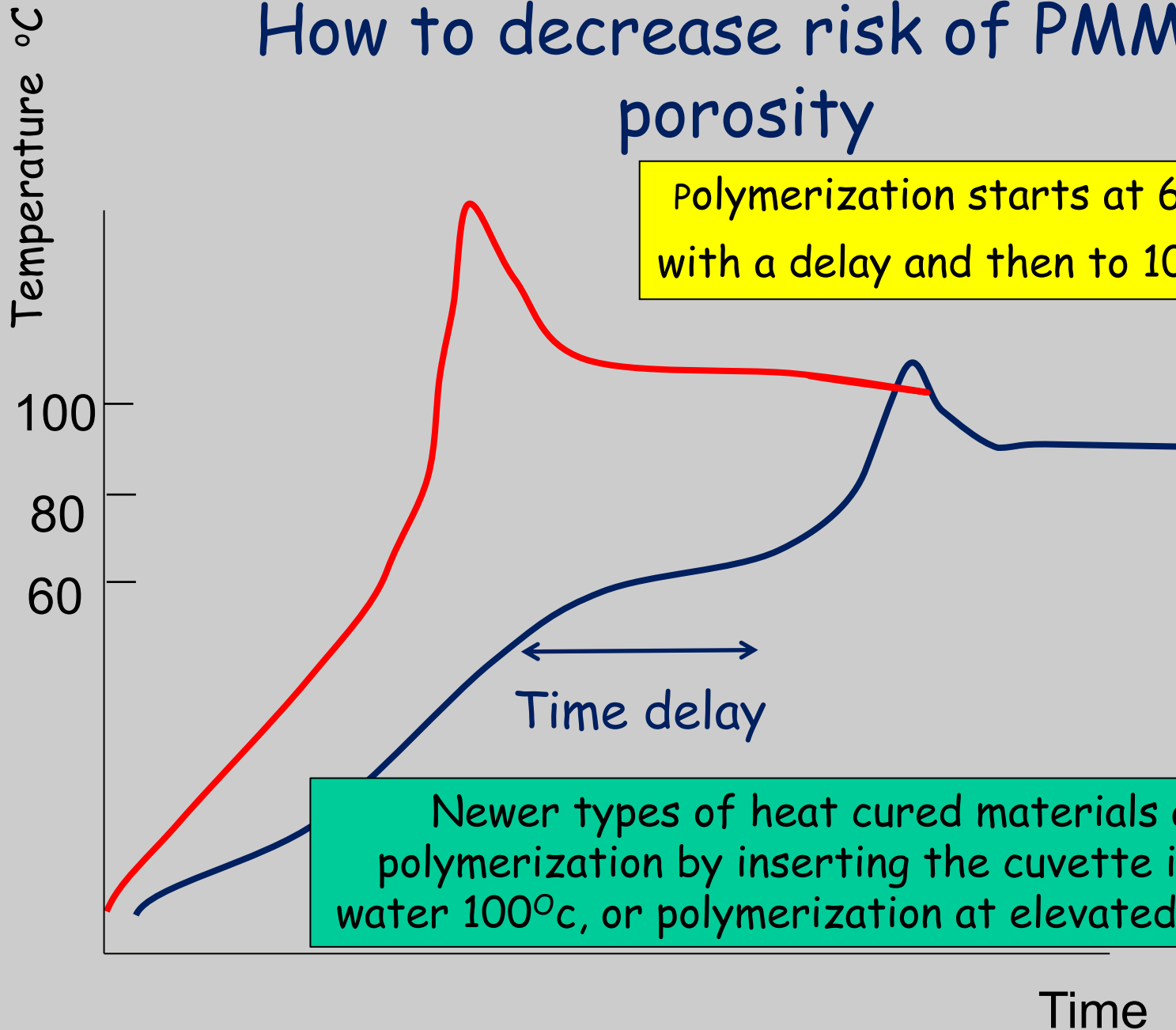


# Autoacceleration/gel effect



# How to decrease risk of PMMA porosity

Polymerization starts at 60°C with a delay and then to 100°C

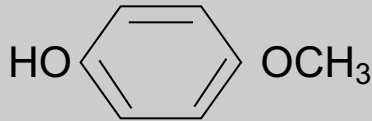


# Phenolic retarders/inhibitors

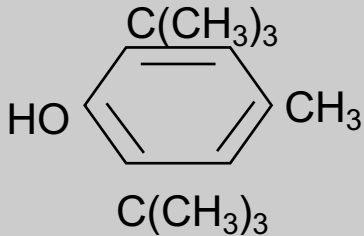


hydroquinone (HQ)

Stable hydroquinone radicals will not propagate and **thus stops** polymerization



methoxy phenol 4-MP, hydroquinone monomethyl ether, MEHQ



2,6-di-tertbutyl-4-methylphenol  
(butylated hydroxytoluene - BHT)

1. Sterically hindered phenols BHT, 4-MP **are less efficient** than HQ but reduce **colour change of polymers** due to oxidation products of HQ.
2. Therefore synergetic mixtures HQ + 4-MP, 4-MP+BHT are now more frequently used.

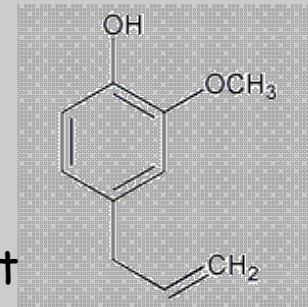
# Why polymer inhibitors are added?

Usually 0.01 - 0.005 wt. %

1. To extend monomer shelf-life by preventing spontaneous polymerization
2. To prolonge the working time
3. To decrease sensitivity of monomers to ambient light (light cured composite materials)

## Note

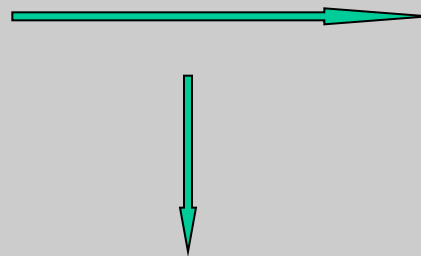
1. Eugenol = phenol  
(inhibits polymerisation)



4-Allyl-2-methoxyphenol

Zinc oxide-eugenol cements-may negatively affect or stop setting of composite materials

## 2. Oxygen inhibition



Stable hydroperoxid

Oxygen-inhibited layer on the  
composite/adhesive surfaces

# Chemically activated resins

(denture repair materials, relining materials, orthodontic appliances, pouring resins)

Composition:

**powder:** PMMA prepolymer or copolymer (fine particle size), residual dibenzoyl peroxide in the PMMA beads, app. 0.5 - 0.6 wt %)

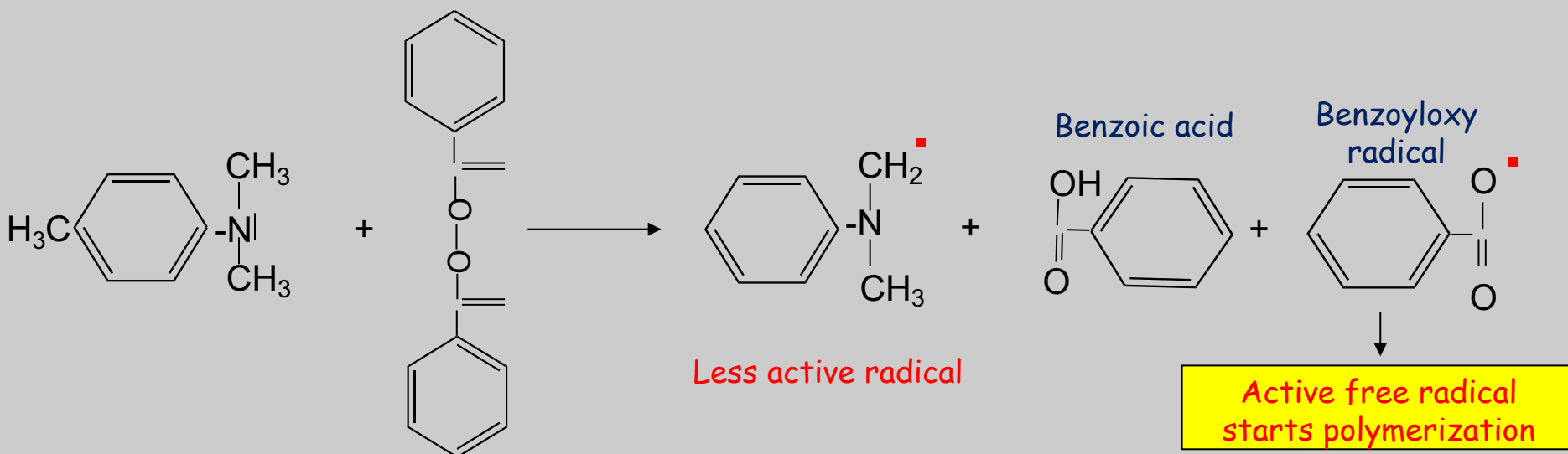
**liquid:** MMA, crosslinking agents, acclerators (1-4 wt%), inhibitors, UV absorbers

## Acclerators

1. Tercial aromatic amine
2. Barbituric acid derivatives combined with aliphatic amine (lower color change) and Cu salts
3. Sodium p-toluene-sulfinat (for systems containing methacrylic acid)



## Scheme of DBP decomposition accelerated by tertiary aromatic amine



N,N-dimethyl-p-toluidine (DMPT); N,N-di(hydroxyethyl)-p-toluidine

### Compared to heat activated resins:

- Lower molecular weight
- Higher amount of free monomers 3-5 wt %, heat activated app. up to 1 %
- Less color stability due to oxidation of aromatic amine accelerators - yellow/brown coloring

For dental applications PMMAs are often modified by:

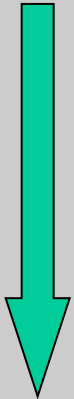
## Cross-linking

- improves hardness and stiffness,
- increases thermal resistance (polymers are easily finished - grinded and polished without melting),
- improves wear and solvent resistance but increases brittleness,
- increases crazing resistance (small cracks originating at the teeth-denture margin).

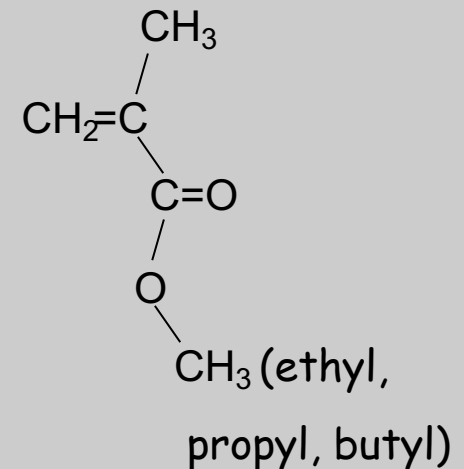
# Copolymerization (e.g. with acrylic and methacrylic monomers, *butadiene*) mainly to avoid leaching of plasticizers

Long side substituent disturbs regular intermolecular order of a homopolymer - decrease in  $T_g$

rigid



Methacrylate	Polymer $T_g$ °C
methyl	125
ethyl	65
n-propyl	38
n-butyl	33



Soft, faster  
dissolution

- decreases softening temperature
- improves fatigue and impact resistance
- increases dissolution rate in MMA

## **Blending** of various acrylic/methacrylic polymers

- increases rate of dissolution in MMA
- decreases softening temperature

# Plasticizing

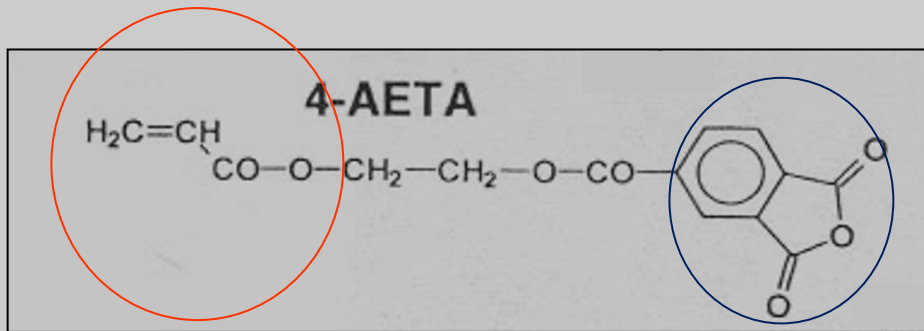
- to reduce stiffness and hardness,
- to prepare flexible polymers (acrylic relining materials)

## Plasticizers

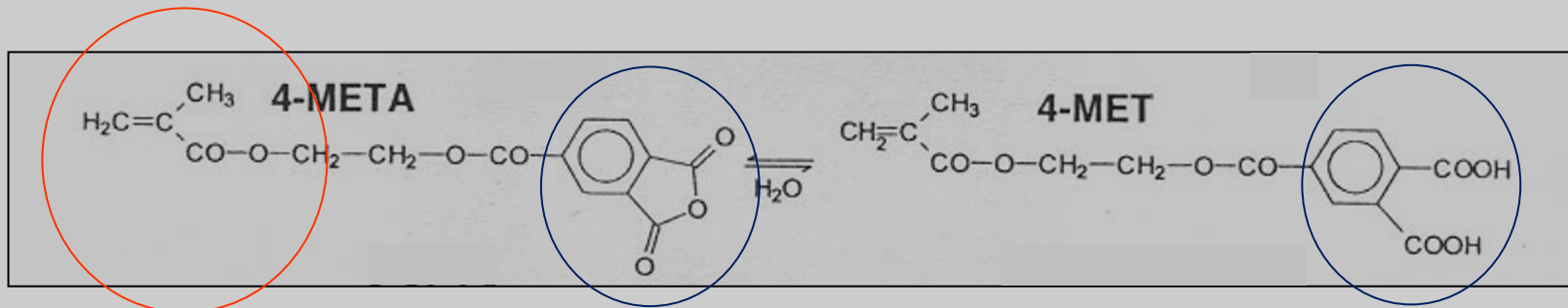
high-boiling point compounds swell polymers  
(phthalates - dibutyl/dioctyl phthalates) - leachable  
potentially harmful

Currently - not frequently used

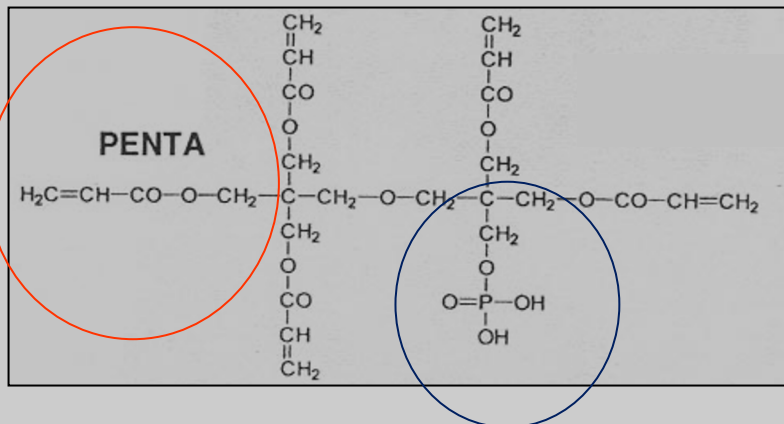




4-acryloxyethyl trimellitic acid anhydride



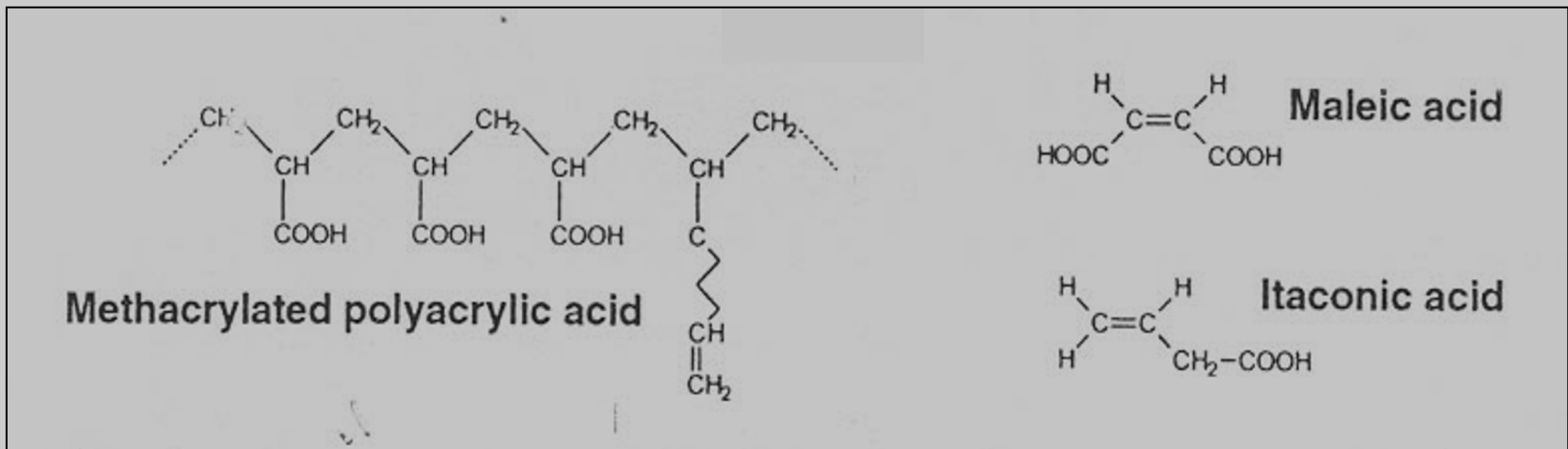
4-methacryloxyethyl trimellitic acid anhydride/acid



Dipentaerythritol penta acrylate monophosphate

# Multifunctional polymers and monomers

Similar principles of free radical polymerization as for monomers with a single MMA unit



Polyacrylic acid with pendant methacrylate groups used in hybrid glass-ionomer cements

Multifunctional monomers in composite formulation



# Summary

1. Polymers, characterization, properties (molecular structure)
2. Chain-growth polymerization (free radical); step-growth (polycondensation and polyaddition)
3. Phases of free radical polymerization
4. Properties of MMA, polymerization of PMMA
5. Inhibitors
6. Characteristics of heat, chemical and light activation systems
7. Dimethacrylate resins used in composite materials
8. Other monomers and polymers in dentistry

# Literature:

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- Powers JM., Sakagushi RL: Craig's Restorative Dental Materials, Mosby
- Gladwin M., Bagby M.: Clinical Aspects of Dental Materials, Theory, Practice and Cases, Lippincott Williams/Williams
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